

The Implementation of a Second Source for Electron Beam Refined Nitinol (HCF-SE) using Fort-Wayne-Metals Vacuum-Arc-Remelted Ingots

by Admedes GmbH, Fort Wayne Metals, Euroflex GmbH, G.RAU GmbH & Co KG, Meko Manufacturing e.K., Vascotube GmbH

Introduction

In the medical device industry Nitinol is a main material for various applications like stents and heart valve frames that are made from Nitinol tubing. The number of Nitinol ingot suppliers is limited and Fort Wayne Metals (FWM) extended their melting capacity to supply Nitinol bar for tube manufacturing.

Consequently, the cooperative project PRIME (PRoficient Ingot Material Evaluation) was started driven by a collective of industry leaders along the process chain. The collective consists of the melt supplier Fort Wayne Metals, continuing along the process chain with Nitinol tube manufacturers Vascotube and Euroflex and finally medical device contract manufacturers MeKo and Admedes. This collaborative project is dedicated to evaluate the new Nitinol source for tube processability and device manufacturing requirements.

The project includes different melting methods resulting in different material grades as well as different tube sizes. This part of the whitepaper focused on so called GEN III Material. Generation I Nitinol Vacuum Arc Remelt (VAR) ingot material is used as a base material for Electron Beam Refinement (EBR) resulting in Generation III material, known as HCF-SE.

Keywords: VAR, EBR, Tube, Component



1 VAR-EBR INGOT

At G.Rau GmbH several VAR ingots were refined using FWM ASTM F2063 conform pre-material ingots. Heat 337464 was used for the following investigations that met the full requirements of ASTM F2063. A summary of the chemical requirements and analysis is shown in Table 1.

Element in % (mass/ mass)	ASTM F2063	337464
Ni	54.5 to 57.0	55.3
C, max.	0.040	0.001
Co, max.	0.050	0.004
Cu, max.	0.010	0.0017
Cr, max.	0.010	0.0033
H, max.	0.005	0.0009
Fe, max.	0.050	0.018
Nb, max.	0.025	0.002
N, max.	0.005	0.003
O, max.	0.040	0.021

Table 1: Chemical composition requirements and analysis.

Figure 1 is one differential scanning calorimetry (DSC) curve of heat 337464 in fully annealed condition. The corresponding Austenitic start (As) transformation temperature is -28 °C and Austenitic finish (Af) temperature is -15 °C. The As transformation temperature range requirement of ASTM F2063 specifying a maximum range of 20 °C is fulfilled.

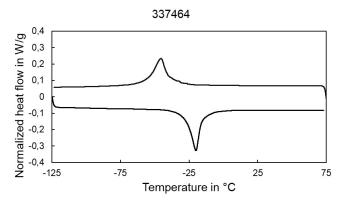
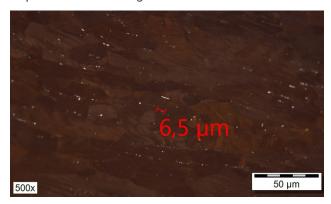


Fig. 1: Differential scanning calorimetry of fully annealed heat 337464.

Figure 2 is a representative micrograph of HCF mill product in annealed condition showing the inclusion size satisfied the ASTM F2063 requirements and HCF-SE specification (see Table 2). In addition, the ASTM grain size number 9 of the mill product fulfilled ASTM F2063 requirement of ASTM grain size number 4 or finer.



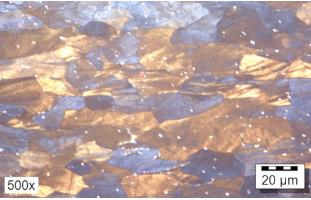


Fig. 2: Micrograph of mill product (337464) for inclusion (upper) and grain size analysis (lower).

	VAR-EBR specification	337464
Max. inclusion	10 μm	8.3 µm
Max. area fraction	0.7 %	0.5 %

Table 2: Inclusion size VAR-EBR ingot



2 TUBE MANUFACTURING

Part II: Nitinol Ingot for HCF-SE, Rev.1

Two different tube sizes were manufactured from Euroflex according to standard specifications (Table 3). Each manufactured tube batch was shipped to medical device contract manufacturers Admedes and MeKo. Both medical device contract manufacturers conducted incoming inspection by examining the microstructure and mechanical properties on the incoming tube from each batch.

Specification	Size 1	Size
Tube size	7 x 0.50 mm	4 x 0.10 mm
UTS min	1100 MPa	1100 MPa
UPS min (3%)	380 MPa	380 MPa
Elongation at	12 %	12 %
fracture min		
Residual elongation	Max. 0.3 %	Max. 0.3 %
after 6 %		
Af max.	15 °C	15 °C

Table 3: Tube specifications

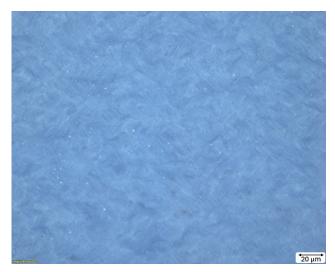
Max. inclusions	7.0x0.50 mm	4.0x0.1 mm
Admedes	2 µm	7 μm
MeKo	5 μm	2 µm

Table 4: Max. inclusion size VAR-EBR tubing.

Area fraction	7.0x0.50 mm	4.0x0.1 mm
Admedes	0.08 %	0.23 %
МеКо	0.09 %	0.01 %

Table 5: Area fraction VAR-EBR tubing.

Figure 3 and Figure 4 show the microstructure of the finished tubing in the longitudinal direction. The focus of this analysis was to understand, if stringers were formed during the tube manufacturing process as a consequence of cold forming steps. No stringers and voids were observed at 500x magnification.



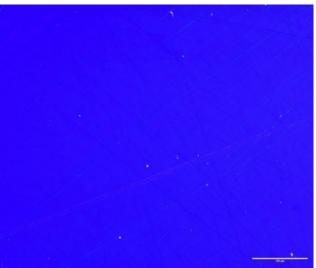


Fig. 3: Inclusion analysis of 7x0.5 tube in longitudinal direction using 500x magnification. Upper: Analysis by Admedes. Lower: Analysis by MeKo.



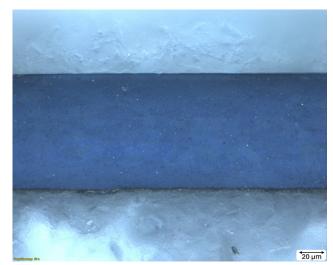




Fig. 4: Inclusion analysis of 4x0.1 tube in longitudinal direction using 500x magnification. Upper: Analysis by Admedes. Lower: Analysis by MeKo.

Admedes and MeKo used a dogbone-shaped geometry (see Figure 5) to perform mechanical testing of tubes according to ASTM F2516. Admedes ran the tests at room temperature (22 °C) and MeKo at body temperature (37 °C). Resulting tensile test diagrams for 7x0.5 tubing are shown in Figure 6 and for 4x0.1 tubing in Figure 7. A summary of mean mechanical properties including results from G. Rau are listed in Table 5. In contrast to the dogbone sample geometry having a 0.5 mm thin strut width, Euroflex tested full circumference tube samples. Each company used its own test conditions. The differences observed align with the expectations.

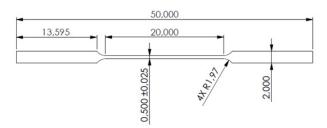
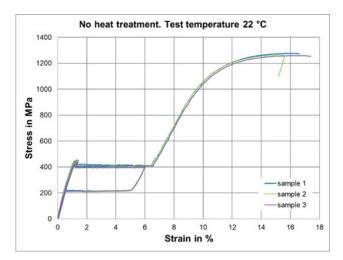


Fig. 5: Geometry of dogbone used for tension testing



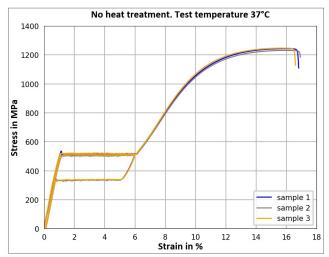


Fig. 6: Tensile test results 7x0.5 mm tube. Upper: Admedes at 22 °C. Lower: MeKo at 37 °C.

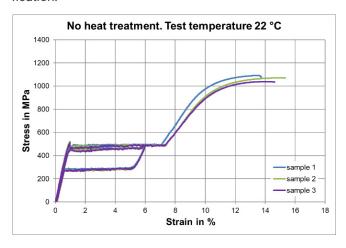


Mech. Properties	UTS in MPa	UPS in MPa	LPS in MPa	Ef in %
7x0.5 tube				
Admedes 22 °C	1266	412	214	16.4
MeKo 37 °C	1241	517	336	16.8
4x0.1 tube				
Admedes 22 °C	1067	479	279	14.6
MeKo 37 °C	1083	557	353	12.6
Euroflex 22 °C	1134	491	261	22.8

Table 6: Average tube mechanical properties.

The transformation temperature was measured at Euroflex using the so-called crush method. It is based on ASTM F2082. A tube section approximately 5 mm long was cooled down in an alcohol bath to -55 °C, the section was crushed into an oval but did not exceed 3 % strain. The bath was heated up to 20 °C with 5° C/min. The Af was determined using the same tangent line method as described in ASTM F2082.

The test results of each condition met the tube specification.



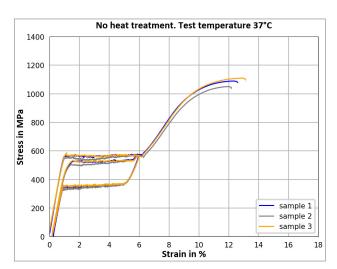


Fig. 7: Tensile test results 4x0.1 mm tube. Upper: Admedes at 22 °C. Lower: MeKo at 37 °C.

Active Af Temperture	7x0.5 mm	4x0.1 mm
Admedes	-7.3	-20.4
MeKo	-7.4	-20.0

Table 7: Transformation temperature of tubes.

3 COMPONENT MANUFACTURING

Admedes and MeKo used the HCF-SE Nitinol tubing to evaluate the material in the component manufacturing process chain by producing generic heart valve frames and neuro stents. For the generic heart valve frames shown in Figure 8 the tube size of 7x0.5 was used while for the neuro stents shown in Figure 9 the tube size of 4x0.1 was processed. Both manufacturers used their standard process chains including laser cutting, heat treatment, and surface removal processes.

In total, MeKo and Admedes manufactured 44 heart valve frames. At both contract manufacturers there were no complications during laser cutting, heat treatment, or surface processes.



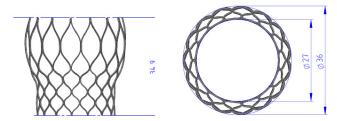


Fig. 8: Generic heart valve frame design in front and top view

In addition, 40 generic neuro stents were manufactured. Both device contract manufacturers observe high scrap rates due to varying geometry like inconstant strut width. The higher scrap rate can be attributed to high residual stresses in the Nitinol tube due to a high diameter-wall thickness-ratio and is not heat related.

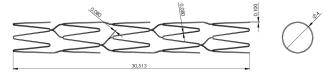


Fig. 9: Neuro stents frame design in front and top view

3.1 Surface

The surface of the heart valve frames and neuro stents were inspected by light microscope and scanning electron microscope (SEM).

Representative pictures of the heart valve frames of the outer diameter, inner diameter, and tip ends are shown in Figure 10. In summary, there were no material related defects observed at either contract manufacturer.

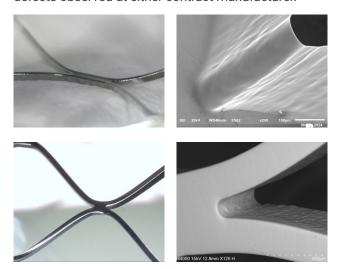


Fig. 10: Light microscope (left) and SEM (right) of heart valve frames. Upper: Admedes. Lower: MeKo.

Representative pictures of the outer diameter and inner diameter of the generic neuro stent design are shown in Figure 11. There were no material related defects observed.

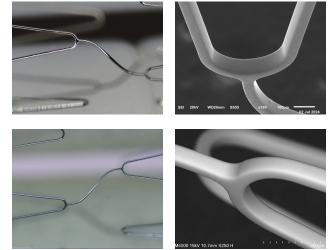


Fig.11: Light microscope (left) and SEM (right) of neuro stents. Upper: Admedes. Lower: MeKo.

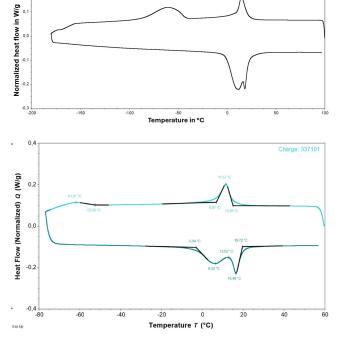


Fig. 12: DSC curves of heart valve frame after heat treatment by Admedes (upper) and MeKo (lower).

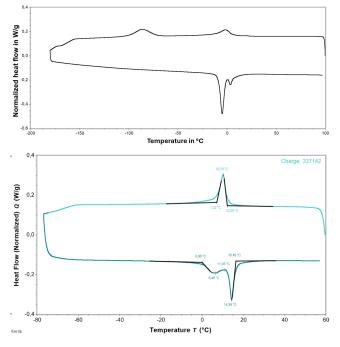


4 DIFFERENTIAL SCANNING CALORIMETRY

DSC tests of the heat-treated components were conducted based on ASTM standard F2004. Each contract manufacturer used their standard temperature range for DSC. For Meko the range is between -80 °C and 60 °C and for Admedes between -180 °C and 100 °C.

The contract manufacturers chose expansion and heat treatment steps independently of each other. The DSC results are shown in Figure 12 and 13 and fulfilled the expectations.

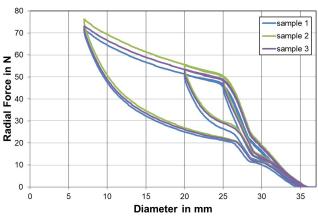
Fig. 13: DSC curves of neuro stents after heat treatment by



Admedes (upper) and MeKo (lower).

5 RADIAL FORCE

The heart valve frames with an outer diameter of 36 mm were crimped in three crimp cycles to a decreasing crimp diameter of 25 mm, 20 mm and 7 mm to determine the radial force. The results are shown in Figure 14. The test results of MeKo (see Figure 14 lower) show a maximum diameter of 30 mm as it is the maximum diameter of the radial force tester. The results met the expectations.



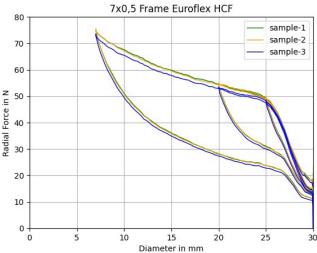


Fig. 14: Radial force tests of herat valve frame by Admedes (upper) and MeKo (lower).



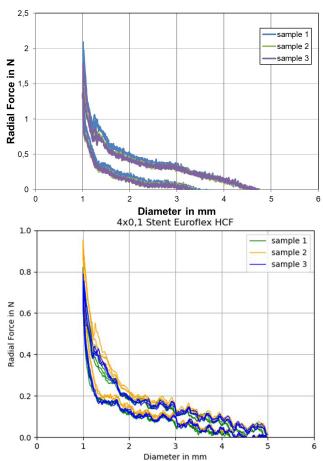


Fig. 15: Radial force tests of neuro stent by Admedes (upper) and MeKo (lower).

The neuro stents with an outer diameter of 4.3 mm were crimped in three crimp cycles to a crimped diameter of 1 mm, see Figure 15. The results met the expectations.

6 CORROSION

The samples were subjected to corrosion testing using cyclic potentiodynamic polarization in phosphate-buffered saline solution at body temperature according to ASTM F2129. A saturated calomel electrode (SCE) was used as the reference electrode. Admedes and MeKo tested at least 5 samples from every material lot. The results of heart valve frames (HVF) and neuro stents are summarized in Table 8 and Table 9. There were either high breakdown potentials over 900 mV or no breakdown (nB) observed, meaning the parts were considered corrosion resistant.

No.	Sample	Er in mV (SCE)	Eb in mV (SCE)	Ev in mV
1	HVF	-238	nB	1000
2	HVF	-402	nB	1000
3	HVF	-401	nB	1000
4	HVF	-375	nB	1000
5	HVF	-389	nB	1000
6	HVF	-231	nB	1000
7	HVF	-408	nB	1000
8	HVF	-433	nB	1000
9	HVF	-389	nB	1000
10	HVF	-434	nB	1000
1	Neuro stent	-352	nB	1000
2	Neuro stent	-329	nB	1000
3	Neuro stent	-264	nB	1000
4	Neuro stent	-259	nB	1000
5	Neuro stent	-267	nB	1000

Table 8: Corrosion test results of heart valve frames and neuro stents by Admedes.

No.	Sample	Er in mV (SCE)	Eb in mV (SCE)	Ev in mV
1	HVF	-401	977	1300
2	HVF	-399	957	1300
3	HVF	-356	962	1300
4	HVF	-276	996	1300
5	HVF	-329	1011	1300
1	Neuro stent	-361	950	1300
2	Neuro stent	-380	997	1300
3	Neuro stent	-407	994	1300
4	Neuro stent	-328	1018	1300
5	Neuro stent	-419	971	1300

Table 9: Corrosion test results of heart valve frames and neuro stents by MeKo.

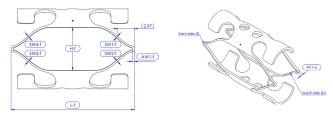


Fig. 16: Diamond fatigue specimen for 7x0.5 mm tubing.



7 FATIGUE TESTS

To prove the material quality of the HCF-SE using FWM GEN I ingot, a diamond fatigue study was conducted. The tests were performed at G.RAU Inc. located in Scotts Valley, California.

Both component manufacturers produced a series of diamonds according to the drawing shown in Figure 16. The diamonds were expanded and heat treated using the same recipe.

For FEA purposes, dogbone specimens were produced using the same heat treatment parameters as for the diamond specimens to collect the data for the FEA analysis. With FEA output it is possible to calculate the stress-strain relationship from the force-displacement data which was collected during the fatigue tests.

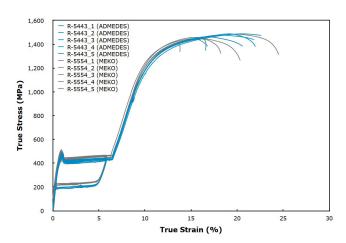


Fig. 17: Tension Test of heat treated dogbones to collect input parameters for FEA.

In addition, the dogbones were used to take DSC measurements to make sure that both series of specimens had the same transformation temperatures (see Table 10).

Lot 700019127 Lot 700019127 Lot 700019127 Lot 700019127 Lot 700019		Nitinol Tensile Dogbone Lot 700019127 (R-5443_1)	Nitinol Tensile Dogbone Lot 700019127 (R-5443_2)	Nitinol Tensile Dogbone Lot 700019127 (R-5443_3)	Nitinol Tensile Dogbone Lot 700019127 (R-5443_4)	Nitinol Tensile Dogbone Lot 700019127 (R-5443_5)
Rρ 11.5 11.9 11.3 11.6 12.3 Rr 6.8 6.8 5.9 6.4 7.5 Ms -47.7 -47.8 -47.1 -47.6 -47.2 Ms -66.7 -67.1 -67.0 -67.2 -66.7 Mr N/A N/A N/A N/A N/A R° -4.4 -3.6 -3.3 -3.3 -3.9 Aρ 17.2 18.6 18.8 18.8 18.8 18.8 Aγ 17.2 18.6 18.8 18.8 18.8 18.8 18.8 18.8 18.8 18.8 18.8 18.8 18.8 18.8 18.8 18.8 18.8 18.8 18.8 18.8<	Transformation Step			Temperature (°C)		
Rt 6.8 6.8 5.9 6.4 7.5 Mb 4.7.7 4.7.8 4-7.1 4.7.6 4.7.3 Mb 4.7.7 4.7.8 4-7.1 4.7.6 4.7.3 Mb N/A N/A N/A N/A N/A N/A Mr N/A N/A N/A N/A N/A N/A R° -4.4 -3.6 -9.3 -9.1 8.2 Ap 17.5 8.6 9.5 9.1 8.2 Ap 21.0 22.5 22.8 22.7 21.9 Transformation Enthalpy (7/9) R 3.3 3.4 3.8 13.8 13.5 13.3 M N/A N/A N/A N/A N/A N/A R/A 13.1 13.5 13.8 13.3 13.3 13.3 13.3 13.3 13.3 13.3 13.3 13.3 13.3 13.3 13.3 13.3 <td>Rs</td> <td>15.3</td> <td>16.0</td> <td>15.5</td> <td>15.7</td> <td>16.0</td>	Rs	15.3	16.0	15.5	15.7	16.0
Ms -47.7 -47.8 -47.1 -47.6 -47.3 Mg -66.7 -67.1 -67.0 -67.2 -66.7 Mr N/A N/A N/A N/A N/A R's -4.4 -3.6 -3.3 -3.3 -3.3 R'g 7.5 8.6 9.5 9.1 8.2 Aθ 21.0 22.5 22.8 22.7 21.9 Transformation Enthalpy (J/g) R 3.3 3.4 3.4 3.4 3.3 M N/A	Rp	11.5	11.9	11.3	11.6	12.3
Mg -66.7 -67.1 -67.0 -67.2 -66.7 Mf N/A N/A N/A N/A N/A Rg 7.5 8.6 9.5 9.1 8.2 Aφ 17.2 18.6 18.8 18.8 18.3 Aγ 21.0 22.5 22.8 22.7 21.9 Transformation Enthalpy (2/y) R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A R/A 13.1 13.5 18.1 13.5 13.3 <td< td=""><td>Rr</td><td>6.8</td><td>6.8</td><td>5.9</td><td>6.4</td><td>7.5</td></td<>	Rr	6.8	6.8	5.9	6.4	7.5
Mr	Ms	-47.7	-47.8	-47.1	-47.6	-47.3
R's 4.4,4 -3.6 -3.3 -3.3 -3.9 R'p 7.5 8.6 9.5 9.1 8.2 Aφ 17.2 18.6 18.8 18.8 18.8 Aγ 21.0 22.5 22.8 22.7 21.9 Transformation Enthalpy (3/g) R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A R'/A 3.1 13.5 13.8 13.5 13.3 Hilled Translet Dopolous (re '9442_1) N/Incell Translet Dopolous (re '9442_2) N/Incell Translet Dopolous (re '	Mρ	-66.7	-67.1	-67.0	-67.2	-66.7
Rγρ 7.5 8.6 9.5 9.1 8.2 Aρ 17.2 18.6 18.8 18.8 18.3 Ar 21.0 22.5 22.8 22.7 21.9 Enthalpy (J/g) R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A R/A 13.1 13.5 13.8 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.7 16.0 2.2 2.4 2.2 15.5 15.7 16.0 15.5 15.7 16.0 12.3 3.4 3.4 3.4 3.4 3.4 3.4 <td>Mf</td> <td>N/A</td> <td>N/A</td> <td>N/A</td> <td>N/A</td> <td>N/A</td>	Mf	N/A	N/A	N/A	N/A	N/A
Ap	R's	-4.4	-3.6	-3.3	-3.3	-3.9
Transformation Tra	R'p	7.5	8.6	9.5	9.1	8.2
Transformation Section Sectio	Ap	17.2	18.6	18.8	18.8	18.3
R 3.3 3.4 3.4 3.4 3.4 3.3 M N/A	Ar	21.0	22.5	22.8	22.7	21.9
M N/A 13.1 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.3 13.5 13.	Transformation			Enthalpy (J/g)		
R/A 13.1 13.5 13.8 13.5 13.5 13.8 13.5 13.8 13.5 13.8 13.5 13.8 13.5 13.8 13.5 13.8 13.5 13.8 13.5 13.8 13.5 13.8 13.5 13.8 13.5 13.8 13.5 13.8 13.5 13.8 13.5 13.8 13.5 13.8 13.5	R	3.3	3.4	3.4	3.4	3.3
Part	М	N/A	N/A	N/A	N/A	N/A
Transformation Step (xx 7 9001912) / (xx 444,2) (xx 7 9001912) / (xx 444,2) (xx 7 9001912) / (xx 444,2) (xx 444,2) (xx 44,2) <td>R'/A</td> <td>13.1</td> <td>13.5</td> <td>13.8</td> <td>13.5</td> <td>13.3</td>	R'/A	13.1	13.5	13.8	13.5	13.3
Rs 15.3 16.0 15.5 15.7 16.0 Rp 11.5 11.9 11.3 11.6 12.3 Rr 6.8 6.8 5.9 6.4 7.5 Ms -47.7 -47.8 -47.1 -47.6 -47.2 Mp -66.7 -67.1 -67.0 -67.2 -66.7 Mr N/A N/A N/A N/A N/A Rs -4.4 -3.6 -3.3 -3.3 -3.3 -3.9 Rp 7.5 8.6 9.5 9.1 8.2 8.8 18.8 18.3 Ar 21.0 22.5 22.8 22.7 21.9 21.		Lot 700019127	Lot 700019127	Lot 700019127	Lot 700019127	Nitinol Tensile Dogbone Lot 700019127 (R-5443_5)
Rp 11.5 11.9 11.3 11.6 12.3 Rr 6.8 6.8 5.9 6.4 7.5 Ms -47.7 -47.8 -47.1 -47.6 -47.3 Mp -66.7 -67.1 -67.0 -67.2 -66.7 Mr N/A N/A N/A N/A N/A Rs -4.4 -3.6 -3.3 -3.3 -3.9 Rp 7.5 8.6 9.5 -9.5 9.1 8.2 Ap 17.2 18.6 18.8 18.8 18.3 Ar 21.0 22.5 22.8 22.7 21.9 Transformation Entalpy (7/y) R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A	Transformation Step			Temperature (°C)		
Rr 6.8 6.8 5.9 6.4 7.5 Ms -47.7 -47.8 -47.1 -47.6 -47.3 Mp -66.7 -67.1 -67.0 -67.2 -66.7 Mr N/A N/A N/A N/A N/A Rs -4.4 -3.6 -3.3 -3.3 -3.3 -3.9 Ap 17.2 18.6 18.8 18.8 18.8 18.3 Ar 21.0 22.5 22.8 22.7 21.9 Transformation Enthalpy (J/g) R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A	Rs	15.3	16.0	15.5	15.7	16.0
Ms -47.7 -47.8 -47.1 -47.6 -47.3 Mp -66.7 -67.1 -67.0 -67.2 -66.7 Mr N/A N/A N/A N/A N/A R's -4.4 -3.6 -3.3 -3.3 -3.9 R'p 7.5 8.6 9.5 9.1 8.2 Ap 17.2 18.6 18.8 18.8 18.3 Ar 21.0 22.5 22.8 22.7 21.9 Transformation R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A	Rp	11.5	11.9	11.3	11.6	12.3
Mp -66.7 -67.1 -67.0 -67.2 -66.7 Mr N/A N/A N/A N/A N/A R's -4.4 -3.6 -3.3 -3.3 -3.9 R'p 7.5 8.6 9.5 9.1 8.2 Ap 17.2 18.6 18.8 18.8 18.3 Ar 21.0 22.5 22.8 22.7 21.9 Transformation Enthalpy (Jy) R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A	Rr	6.8	6.8	5.9	6.4	7.5
Mr N/A N/A N/A N/A N/A R's -4.4 -3.6 -3.3 -3.3 -3.9 R'p 7.5 8.6 9.5 -9.1 8.2 Ap 17.2 18.6 18.8 18.8 18.8 Ar 21.0 22.5 22.8 22.7 21.9 Transformation R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A	Ms	-47.7	-47.8	-47.1	-47.6	-47.3
R's .4,4 -3,6 -3,3 -3,3 -3,9 R'p 7,5 8.6 9,5 9,1 8,2 Ap 17,2 18,6 18,8 18,8 18,3 Ar 21,0 22,5 22,6 22,7 21,9 Transformation R 3,3 3,4 3,4 3,4 3,3 M N/A N/A N/A N/A N/A	M _p	-66.7	-67.1	-67.0	-67.2	-66.7
R'p 7.5 8.6 9.5 9.1 8.2 Ap 17.2 18.6 18.8 18.8 18.3 Ar 21.0 22.5 22.8 22.7 21.9 Transformation R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A	Mf	N/A	N/A	N/A	N/A	N/A
Ap 17.2 18.6 18.8 18.8 18.3 Ar 21.0 22.5 22.8 22.7 21.9 Entalpy (7/9) R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A N/A	R's	-4.4	-3.6	-3.3	-3.3	-3.9
Ar 21.0 22.5 22.8 22.7 21.9 Transformation Enthalpy (J/g) R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A N/A	R'p	7.5	8.6	9.5	9.1	8.2
Transformation Enthalpy (3/g) R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A N/A	Ap	17.2	18.6	18.8	18.8	18.3
R 3.3 3.4 3.4 3.4 3.3 M N/A N/A N/A N/A N/A N/A	Ar	21.0	22.5	22.8	22.7	21.9
M N/A N/A N/A N/A N/A	Transformation			Enthalpy (J/g)		
R'/A 13.1 13.5 13.8 13.5 13.3	R	3.3	3.4	3.4	3.4	3.3

Table 10: DSC Tests of heat-treated dogbones to show equivalency of both sets of diamonds. Upper: Admedes. Lower: Meko.

The test conditions are summarised in Table 11.

Test Conditions	Pre-Strain
Pre-Strain	9 %
Mean Strain	3 % and 5 %
Strain Amplitude	2.0 % and 3.0 %
Test Temperature	37 °C
Test Frequency up to 1000 cycles	1 Hz
Test Frequency up to 10 Mio cycles	25 Hz
Test Specimens per condition per	5
component manufacturer	

Table 11: Test conditions fatigue setup.

There were zero fractures observed under the 2 % strain amplitude-test conditions listed in Table 11. This result is in line with the reported tests using another VAR material supplier as pre-material for the HCF-SE refining process. Since this test was designed for test to fracture, the 3 % strain amplitude condition was added. All specimens had at least one fracture after 10 million cycles. Figure 18 also shows the current fatigue strain limit line for Gen I as a comparison. This means that the fatigue strain limit of HCF-SE was about 4 to 5 times higher than Gen I Nitinol material.



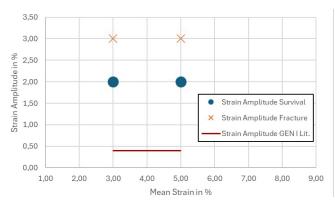


Fig. 18: Fatigue results diamond testing till 10 million cycles.

8 CONCLUSION

Within the context of the PRIME project Gen I Nitinol was supplied by Fort Wayne Metals and further processed using EBR by Euroflex. The objective was to verify whether the material functions effectively in the processes of each company along the process chain and whether the resulting products meet the quality requirements. Multiple Nitinol HCF tube sizes were manufactured. In this whitepaper tubes with an outer diameter of 7 mm and wall thickness of 0.5 mm, as well as an outer diameter of 4 mm and wall thickness of 0.1 mm were investigated and further processed to heart valve frames or neuro stents.

The material investigation began with the melt, which complied with the relevant standard ASTM F2063 and Euroflex internal specifications. The produced bar machinability allowed for gun drilling and subsequent fabrication into tubes. No complications were observed during tube drawing process by Euroflex. The manufactured tubes met all specified mechanical and dimensional requirements. Furthermore, these tubes have been determined to serve as suitable semi-finished product for device manufacturing, with all analyzed results aligning with the expected quality and performance criteria. Specifically, the results of DSC, radial force, and corrosion tests were inconspicuous, and the surface quality meets all quality requirements.

The fatigue specimens were manufactured from the two different 7×0.5 mm tube lots. There were 10 total

specimens tested per condition, 5 from each component manufacturer, with 5 specimens tested under the same condition. Therefore, one datapoint in Figure 18 represents 10 test results from fatigue specimens. Each diamond had eight critical fracture locations. This means that each datapoint represents 80 positions within the material.

Based on the results compiled in this paper, the FWM VAR- material which met ASTM F2063 requirements, is deemed suitable as a base material to make HCF-SE GEN III ingot. The final product made from those ingots show the same performance regarding producibility, material characteristics and fatigue resistance as the currently used VAR base material.

With having two independent sources for VAR pre-material, the EBR process used to make HCF-SE decouples component manufacturers and their clients from instabilities in the ingot supply chain.

Looking ahead, the tube investigations will be extended by Vascotube and Euroflex tube that is undergoing testing at the time of publication.

9 ACKNOWLEDGMENTS

The investigations discussed in this paper were funded by the partners Fort Wayne Metals Research Products, Vascotube a Cirtec Company, Euroflex GmbH, G.RAU GmbH & Co KG, Admedes GmbH and MeKo Manufacturing e.K..



10 REFERENCES

ASTM F2063-18, Standard specification for wrought Nickel-Titanium shape memory alloys for medical devices and surgical implants, ASTM International

ASTM F2516-22, Standard test method for tension testing of Nickel-Titanium superelastic materials, ASTM International

ASTM F2082/F2082M-23, Standard test method for determination of transformation temperature of Nickel-Titanium shape memory alloys by bend and free recovery, ASTM International

ASTM F2004-24, Standard test method for transformation temperatures of Nickel-Titanium alloys by thermal analysis, ASTM International

ASTM F2129-24, Standard test method for conducting cyclic potentiodynamic polarization measurements to determine the corrosion susceptibility of small implant devices, ASTM International